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Biomechanics of the Sacroiliac Joint: Part II—Surgical Treatments

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ABSTRACT

Background: Fixation is one of the most common surgical techniques for the treatment of chronic pain originating from the sacroiliac joint (SIJ). Many studies have investigated the clinical outcomes and biomechanics of various SIJ surgical procedures. However, the biomechanical literature points to several issues that need to be further explored, especially for the devices used in minimally invasive surgery of the SIJ. This study (part II) aims to assess biomechanical literature to understand the existing information as it relates to efficacies of the surgical techniques and the gaps in the knowledge base. Part I reviewed basic anatomy and mechanics of the SIJ joint, including difference between males and females, and causes of pain emanating from these joints.

Methods: A thorough literature review was performed pertaining to studies related to SIJ fixation techniques and the biomechanical outcomes of the surgical procedures.

Results: Fifty-four studies matched the search criteria and were considered for the review. These articles predominantly pertained to the biomechanical outcomes of the minimally invasive surgery with different instrumentation systems and surgical settings.

Conclusions: The SIJ is one of the most overlooked sources of lower back pain. The joint is responsible for the pain in 15% to 30% of people suffering from lower back pain. Various studies have investigated the clinical outcomes of different surgical procedures intended to improve the pain and quality of life following surgery. The data show that these techniques are indeed effective. However, clinical studies have raised several issues, like optimal number and positioning of implants, unilateral versus bilateral placements, adjacent segment disease, implant designs, and optimal location of implants with respect to variations in bone density across the SIJ. Biomechanical studies using in vitro and in silico techniques have addressed some of these issues. Studies also point out the need for additional investigations for a better understanding of the underlying mechanics for the improved long-term surgical outcomes. Further long-term clinical follow-ups are essential as well. This review presents pertinent findings.

Biomechanics

Keywords: biomechanics, sacroiliac joint, low back pain, sacroiliac fixation, minimally invasive, surgical procedures, devices

BACKGROUND

Low back pain (LBP) is the most common reason for primary care visits after the common cold, with approximately 90% of adults being affected by this condition at some point in their lives.^{1,2} Apart from hindering the quality of life of those affected by LBP, if left untreated or improperly diagnosed, patients' work productivity, and subsequently the economy, may be adversely affected. LBP accounts for an annual cost up to 60 billion dollars due to decreased productivity and income, and increased medical expenses.^{3–5}

The majority of LBP originates from the lumbar spine. However, one of the most overlooked sources of LBP is the sacroiliac joint (SIJ) due to its complex

nature.² Recent studies have reported a higher prevalence of the SIJ as a source for LBP, with some reports having estimated that the SIJ is the actual source of pain in 15% to 30% of cases.^{6–8} Increased physicians' awareness of the prevalence of the SIJ as a source of LBP has given rise to an increased clinical suspicion of joint dysfunction as a pain generator. Hence, appropriate planning of treatment strategies is becoming a norm.

Current nonsurgical treatment and pain management strategies include physical therapy, SIJ injections, and radiofrequency ablation. When patients continue to present chronic LBP characteristic of SIJ dysfunction, surgical procedures become the final resort. This review article addresses the

diagnosis of SIJ dysfunction, treatments, surgical techniques, and biomechanics of the SIJ. It builds on the part I review that delineates the basic anatomy, differences between females and males, role of ligaments in providing stability, load sharing among various structures, and the numerous causes of LBP emanating from the SIJ.

DIAGNOSIS OF SIJ DYSFUNCTION

Symptoms of SIJ dysfunction include pain in the lower back, buttock, back of the thigh, and knee. Patients with LBP often experience pain when sitting, when leaning forward, and with an increase in intra-abdominal pressure.⁹ While these pain characteristics are associated with SIJ dysfunction, they are also consistent with other hip and spine conditions, making accurate diagnosis and confirmation of the SIJ as the pain source a rather difficult task.

Due to the complexity of diagnosing the SIJ as the pain source, numerous physical tests are in use, many of which incorporate distraction of the SIJs. Two of the most commonly performed tests are the Gaenslen test and Patrick test, also known as the FABER test.¹⁰ Other provocation tests for assessing SIJ pain include distraction/compression tests, the thigh thrust test, and the sacral thrust test.¹¹ If 3 or more of these tests are positive, then diagnosing the SIJ as the source of pain is acceptable.¹² However, many clinical studies have shown rather inconsistent findings in the success of identifying the pain source to be SIJ dysfunction.^{8,10} Thus to improve reliability, further examinations are achieved through other techniques (eg, radiological studies and diagnostic blocks, or intra-articular injections). Radiological imaging with diagnostic injections, however, have yielded low sensitivities and poor correlations with symptoms.¹⁰ An exception is the high specificity of magnetic resonance imaging in the setting of the seronegative spondyloarthropathies (90%-100%).¹³⁻¹⁵ Diagnostic blocks, on the other hand, are the most reliable methods for diagnosing SIJ pain. These blocks, administered under fluoroscopy, are used to determine if a patient experiences a significant reduction in pain while the anesthetic is active.¹⁶

TREATMENT OF SIJ DYSFUNCTION— SURGICAL TECHNIQUES AND NEED FOR IN VITRO AND IN SILICO STUDIES

Several options exist for treatment of SIJ dysfunction and associated pain, ranging from

conservative to minimally invasive and open surgeries. Nonsurgical management options include physical therapy, steroid injections, radiofrequency ablation, and prolotherapy; these are recommended for the early stages of SIJ dysfunction. Under specific conditions such as patients with leg length discrepancy, only using shoe inserts can help eliminating the discrepancy, consequentially equalizing and decreasing the load distribution across the joints over time.^{10,17} However, when the nonsurgical treatment plans fail to overcome the pain and improve the patient's conditions, surgery (open or minimally invasive) is a viable option.

Open SIJ Fusion

When nonsurgical management strategies fail to reduce patient pain and discomfort due to SIJ dysfunction, surgical measures become an option, beginning with open arthrodesis, or fusion of the SIJ. According to Smith et al,¹⁸ open surgical fusion surgery requires longer operative time and hospital stay and caused greater blood loss. Apart from having less advantageous operative measures, open arthrodesis of the SIJ also showed less superior SIJ pain rating changes over the 12- and 24-month follow-ups, compared with minimally invasive surgical approaches for fusion, described next.

Minimally Invasive SIJ Fusion

Minimal invasive surgeries of the SIJ have become quite common these days. Thus, it is advantageous to understand the general procedure for the design and execution of biomechanical studies. During a minimally invasive SIJ fusion procedure, the patient is administered general anesthesia and lies in the prone position for intraoperative fluoroscopy.^{4,7,19} In general, a long lateral incision of the buttocks is the first step to provide access to the joint. Then the gluteal fascia is penetrated and dissected to reach the outer table of the ilium. A Steinmann pin is passed through the ilium across the SI joint to the middle of the sacrum and lateral to the neural foramen.²⁰ The pin enables a soft tissue protector to slide over it for the bone decortication. Upon removal of the drill, a broach is malleted across the joint to prepare a channel for the first implant and using a pin guidance system allows implant placement. Finally, the incision is irrigated and tissue layers are closed.^{4,7,18,20,21} A large number of fusion implant designs are available on the market. Clinical follow-ups assist in evalu-



Figure 1. Triangular titanium implant with porous coating; lateral approach.²⁵

ating the efficacy of these implants. These clinical follow-ups also highlight some of the mechanical issues that need further exploring using in vitro and in silico studies.

Among the different devices for minimally invasive SIJ fusion, perhaps the iFuse implant system (SI-Bone, Inc, Santa Clara, CA) is the most used at present; this system consists of porous titanium plasma spray-coated triangular titanium implants. The shape, coating, and interference fit of these implants allow for initial stabilization or mechanical fixation, and biological fixation leads to effective stabilization of the joint over time.^{4,18,22} The device's several unique features differentiate it from traditional cages and screws. In these implants, interference fit allows proper fixation, the triangular profile reduces implant rotation, and the porous surface minimizes the implant micromotion and enhances bone ingrowth resulting in better fusion. Biomechanical studies showed that an 8-mm cannulated screw is 3 times weaker in shear and bending than a triangular implant (Figure 1).²³ In this system, no grafts are placed in the SIJ; therefore, all fusions are obtained through the bony ingrowth across the porous coating.²⁴

The SI-LOK SIJ fixation system (Globus Medical, Inc, Audubon, PA) is another minimally invasive surgical SIJ fixation device that places 3 hydroxyapatite-coated screws laterally across the sacroiliac joints (Figure 2). There is an optional bone graft slot inside the screw to enhance fusion.

An optional lag screw thread allows compression force during placement.²⁶

The SIMmetry SIJ fusion system, produced by Zyga Technology, Inc (Minnetonka, MN), is a cannulated titanium implant used with 2 screws (one is an antirotation screw) placed laterally across the SIJ (Figure 3). The cannulated threaded implant and the antirotation screw have diameters of 12.5 mm and 6.5 mm, respectively. There is no bone graft slot in this system, and the bone graft is placed across the articular part of the joint.²⁷

SIFix, developed by NuTech Medical, Inc (Birmingham, AL), is one of the posterior minimally invasive surgical SIJ fixation systems that uses 2 threaded cancellous bone dowels to stabilize the joint. The concept minimizes damage to the ligaments and provides compression to promote fusion/union across the SIJ. Bilateral placements with a single midline incision are also feasible with this design (Figure 4).

The RI-ALTO implant, made by Medtronic, Inc (Minneapolis, MN), is another posterior minimally invasive surgical SIJ fusion system; it uses 2 or 3 threaded screws to stabilize the joint. The procedure is safe and effective in SIJ fusion and reduces surgical morbidity due to its posterior approach (Figure 5).

In conclusion, significantly successful reports of surgical outcomes, patient satisfaction, recovery rate, and implant survivorship, show that minimally invasive procedures have the potential to become



Figure 2. SI-LOK sacroiliac joint fixation system implanted using lateral approach.²⁶

the predominant focus for treating patients with chronic SIJ pain. Furthermore, there are various techniques and different types or designs of SIJ fusion implants. These studies, however, do not elucidate the biomechanical effects of surgical parameters such as number and positioning of implants one may use, unilateral versus bilateral placement, etc.

Another issue is the relationship between sacral bone density and surgical outcomes of the fusion procedures. A review of literature on clinical outcomes of SIJ fixation techniques shows that loosening of the hardware at the sacral side seems to be most common. The implant loosening or failure often occurs due to poor bone quality in the sacrum area.³⁰ Several studies have investigated the relationship between sacral bone density and lumbosacral fusion rate.

These studies have shown up to 45% of sacro-pelvic fixations fail due to S1 screw haloing or pullout. Other studies reported inferior screw pullout strength of the sacral screws in sacral bone with low mineral density.³⁰⁻³²

Several clinical studies have reported serious complications following surgical treatment of unstable posterior pelvic ring injuries using SIJ fixation methods.^{33,34} The reported complications included loss of fixation, loss of function, neurovascular injury, and mal-union.

Placement of ilio-sacral screws into the S1 body has been recommended as the preferred method of fixation by these studies; although sacral dysmorphism and size limitation may prevent fixation of S1 using this method.^{34,35} In such cases, alternative methods become essential, like fixation into the

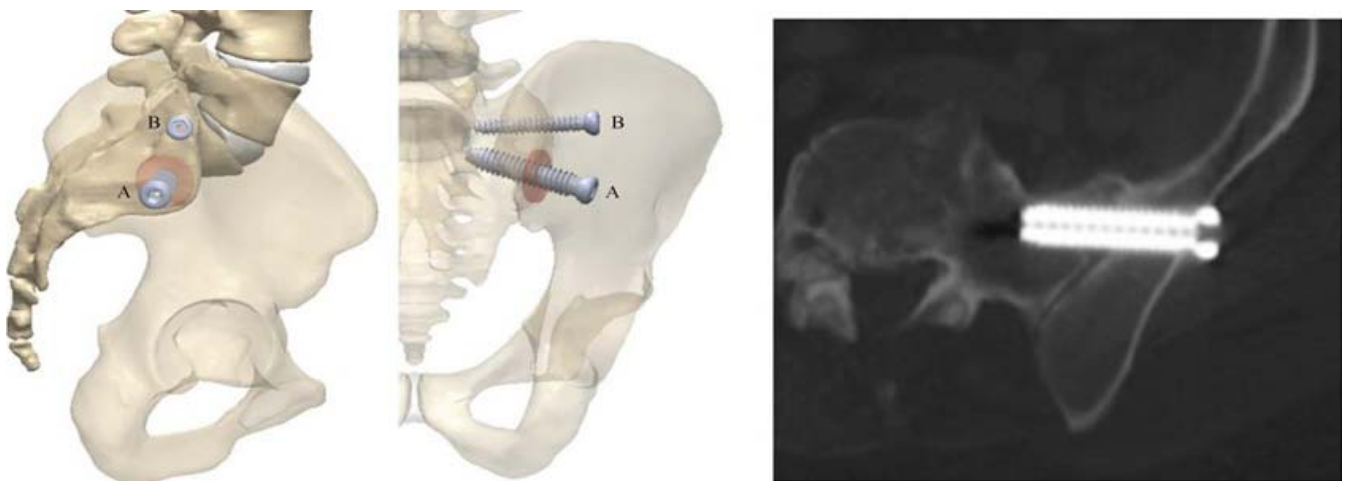


Figure 3. SImmetry sacroiliac joint fusion system; lateral approach.²⁷



Figure 4. SIFix sacroiliac joint fixation system implanted using posterior approach.²⁸

second sacral body (S2).^{36,37} However, the smaller size of the second sacral body results in a decreased tolerance of variant screw trajectories. Thus, achieving a proper fixation into this segment remains the main challenge.^{37,38} The effect of the quality of the surrounding bone in the S2 body on the surgical outcomes are lacking in the literature.

Thus, biomechanical studies using *in vitro* and *in silico* techniques are crucial in addressing the above stated questions.

In Vitro Studies

Soriano-Baron et al³⁹ investigated the effects of placement of triangular implants across the SIJ on range of motion (ROM) versus load for a 1-leg standing posture. Nine fresh frozen specimens were sequentially tested; the intact pubic symphysis was cut to allow the right and left SIJs to move freely following stabilization. Implants were located through the posterior and transarticular approaches. In the posterior procedure, the 3 implants were inline in the inlet view, and parallel in the outlet and

lateral views. In the transarticular approach, the locations of superior and inferior implants were similar to the posterior technique, and the middle implant was located towards the anterior third of the sacrum across the cartilaginous portion of the SIJ. Pure moments up to 7.5 Nm simulated flexion, extension, lateral bending, and axial rotations under the 1-leg stance. Placement of 3 implants in both approaches significantly reduced the ROM in all modes. However, there was no significant difference between these 2 techniques regarding motion reduction.³⁹ The authors extended²² the investigation to study the effects of 5000 cyclic loads on the stabilization characteristics of the fused specimens. The ROM following cyclic loading did not change much, compared precyclic test data.

Lindsey et al²⁵ compared the stabilization characteristics of unilateral and bilateral triangular implant placements across the SIJ during the 1-leg stance condition. Unilateral instrumentation significantly decreased the ROM of the treated side, and did not affect nontreated contralateral SIJ motion

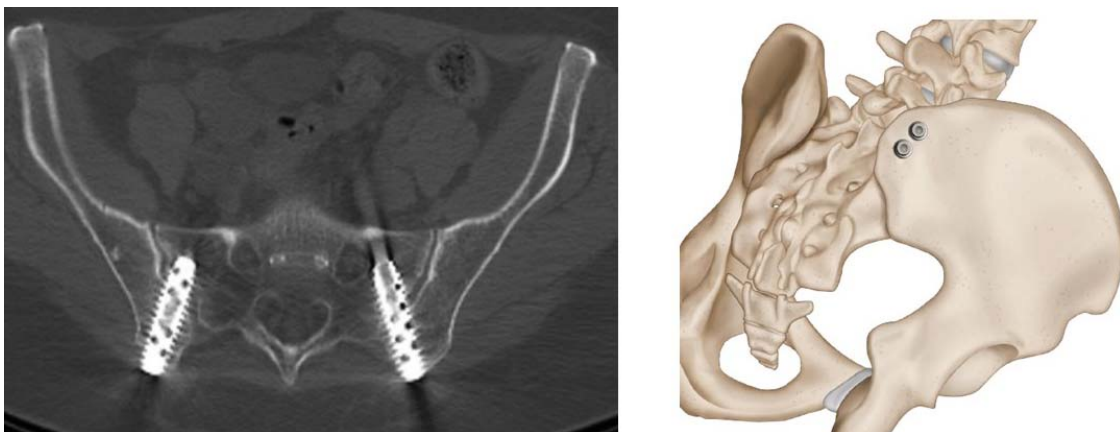


Figure 5. RI-ALTO sacroiliac joint fusion system; posterior approach.²⁹

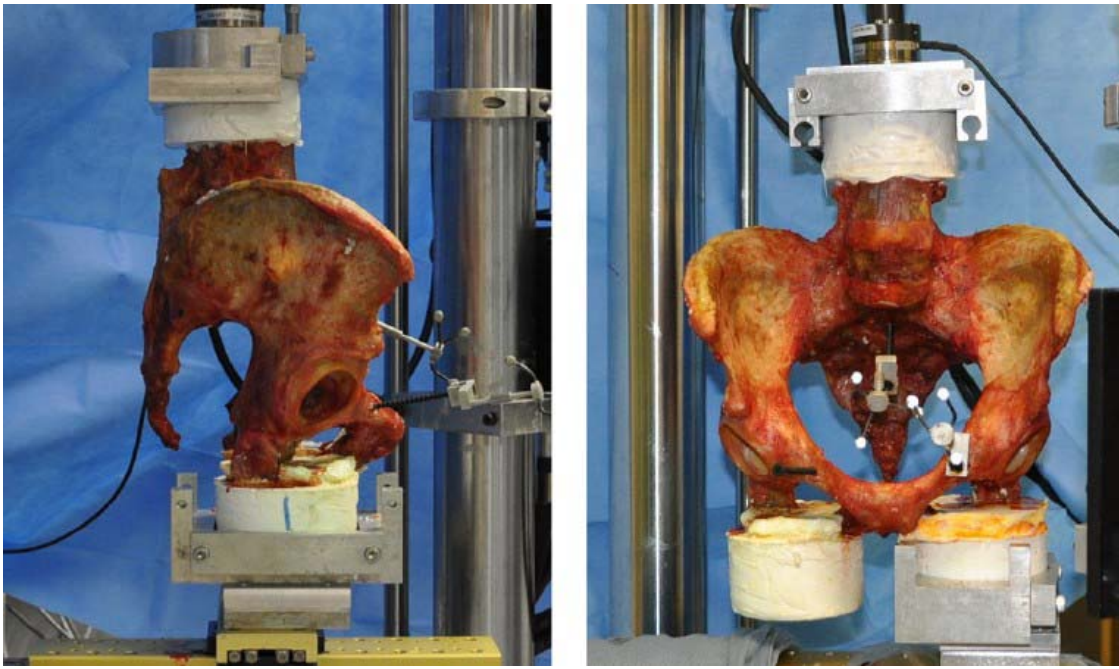


Figure 6. Test setup side view (left) and anterior view (right) under bending moment in materials testing system machine.⁴¹

during the 1-leg stance condition. Bilateral placements reduced motions on both sides. Thus, bilateral instrumentation becomes essential if one wants to reduce the ROM of both of the SIJs.

Jeong et al⁴⁰ assessed the mobility in 3 groups of intact, unilateral, and bilateral fusions using 3 triangular implants in each joint. The loading was pure bending moment of 7.5 Nm under single-leg stance. They observed that unilateral and bilateral SIJ fusions using iFuse implants provided significant reduction in SIJ motions, compared to being intact in all modes.⁴⁰

Shih et al⁴¹ performed an in vitro study to evaluate 2 techniques for placing primary (12.5-mm) and secondary (8.5-mm) threaded rods (Zyga Technology) across the SIJ (Figure 6). They performed cyclic loading after placement of the primary implant at S1 and a secondary implant at either S1 or S2. The fixation using 2 threaded rods significantly reduced SIJ motion and the location of the secondary 8.5-mm implant did not alter construct performance.

Doud⁴² investigated the biomechanics of SIFix fusion technique in a cadaver model. They applied a cyclic compression force ranging from 0.2 to 2.5 times the specimen's body weight for a double-leg stance and 0.6 to 1.8 times the body weight for a single-leg stance to mimic walking. The treated SIJ with SIFix did not provide any reduction in motion following fixation, compared with intact cases.

Recently, a biomechanical study on the SI-Integrity SIJ fusion system was done.⁴³ This implant was similar to Symmetry SIJ fusion. It uses 1 lag screw along with another smaller anti-rotation screw. L4-pelvis specimens were tested intact, destabilized, and instrumented groups in single-leg stance under 7.5 Nm pure moments. The posterior SIJ capsule and ligaments and the pubic symphysis were dissected to destabilize the specimen. They showed that instrumentation significantly reduced the ROM of the joint, compared with the destabilized condition but had similar ROM in flexion/extension and axial rotation, compared with the intact condition.

Lumbar spine fusion, particularly of the L5-S1 segment, affects the biomechanics of the SIJ by increasing both the motion and stresses across its articular surface.⁹ Bariah⁴⁴ determined spinal motions for double- and single-leg stance cases in 4 configurations of intact, L4-L5 fusion, L4-S1 fusion, and unilateral SIJ fixation, using a single 9-mm screw (Figure 7). The effects of body weight and spinal motions were simulated by applying moments (7.5 Nm for torsion and 8.5 Nm for flexion/extension), in addition to preloads. They showed that spinal and lumbosacral fusions led to an increase in SIJ ROM. The SIJs during axial compression, exhibited an increase in anterior motion for the stabilized case as well. The motion at the posterior SIJs increased during all modes of

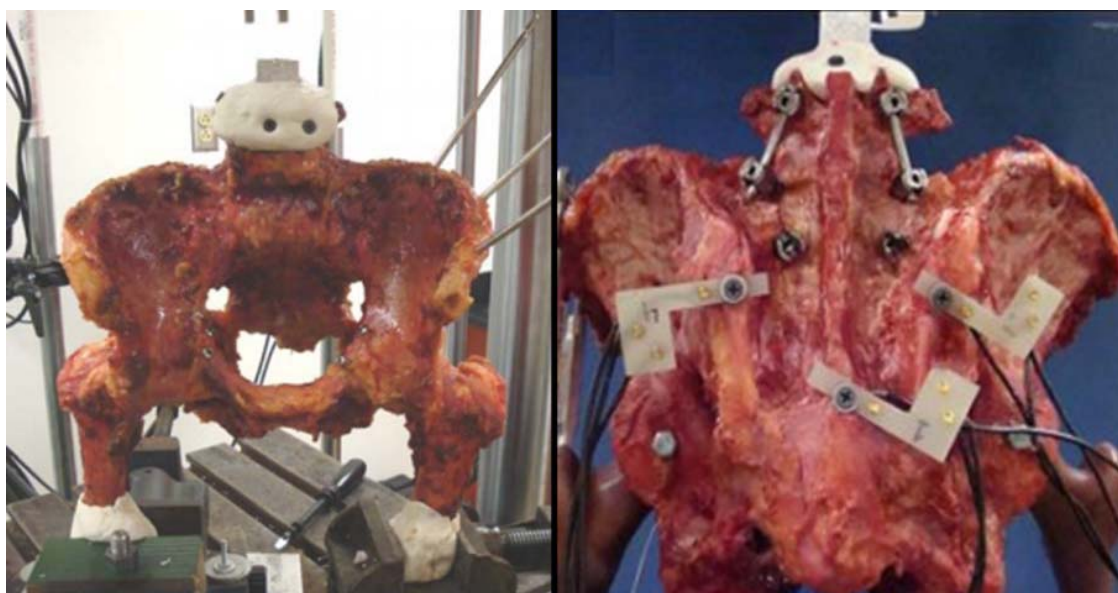


Figure 7. Biomechanical study on intact sacroiliac joint, double-leg stance model (left) and posterior view after L4-L5 fusion (right).⁴⁴

motions (flexion/extension, torsion and axial compression).

In conclusion, *in vitro* studies have shown the efficacy of various implants in reducing the motion across the SIJ. Several questions, such as the mechanism for implant/bone failure, load distribution at bone-implant interface, the location of the critical load, and stresses and strains in the connective tissue and ligaments across the joint remain unanswered. Such limitations necessitate *in silico* modeling to quantify and compare data, using experimentally validated computational models.

In Silico Studies

Several authors have investigated the biomechanics of the SIJ after spinal or SIJ fusion using a computational approach.^{45–47}

Mao et al⁴⁸ investigated the effect of lumbar lordosis alteration on sacrum angular displacement after lumbosacral fusion using finite element analysis. Decreasing and increasing lumbar lordosis resulted in increased sacrum angular motion. In addition, fusion at the L4-S1 level resulted in higher sacrum angular displacement compared with L3-L5-level fusion simulation. This supports the clinical observations that SIJ degeneration incidence is higher in fusions up to S1 rather than L5.

Ivanov et al⁴⁹ evaluated sacrum angular motion and stresses across SIJ after lumbar fusion across L4-L5, L5-S1, and L4-S1 (Figure 8). Fusion resulted in an increase of SIJ motion and stresses across the

SIJ. L4-S1-level fusion led to the highest increases, compared with fusions at other levels.

Bruna-Rosso et al⁵⁰ analyzed SIJ biomechanics for RI-ALTO fusion implants (Figure 9). A compression load (1000 N) to the finite element model to simulate the experimental part of the study. They evaluated the effects of simulating 1 and 2 implants and their placement location across the SIJ. Proximal insertion of the implant placed farther from the SIJ center of rotation was more efficient than its distal insertion location. Proximal insertion of 1 implant even had better performance than using 2 implants in terms of motion reduction. There was not much difference in providing stability between 2 placement trajectories: medial and oblique for 1-implant instrumentation. However, medial placement provided higher stability compared with oblique in 2-implant instrumentation simulation. Overall, the more parallel and farther from the SIJ center of rotation implant placement was, the higher the stability.

Zhang et al⁵¹ studied the biomechanical stability of SIJ screw fixation under 2 types of SIJ dislocations (Figure 10). For each dislocation model, they placed implants at the SIJ in 4 different configurations: a single screw in S1, single screw in S2, 2 screws in S1, and 1 screw in S1 and another single screw in S2. Inferior translation, flexion, and lateral bending data were calculated. In one model, both long and short posterior sacroiliac ligaments were absent and no ligaments were present in the second model. The weakest placement configuration was the single screw

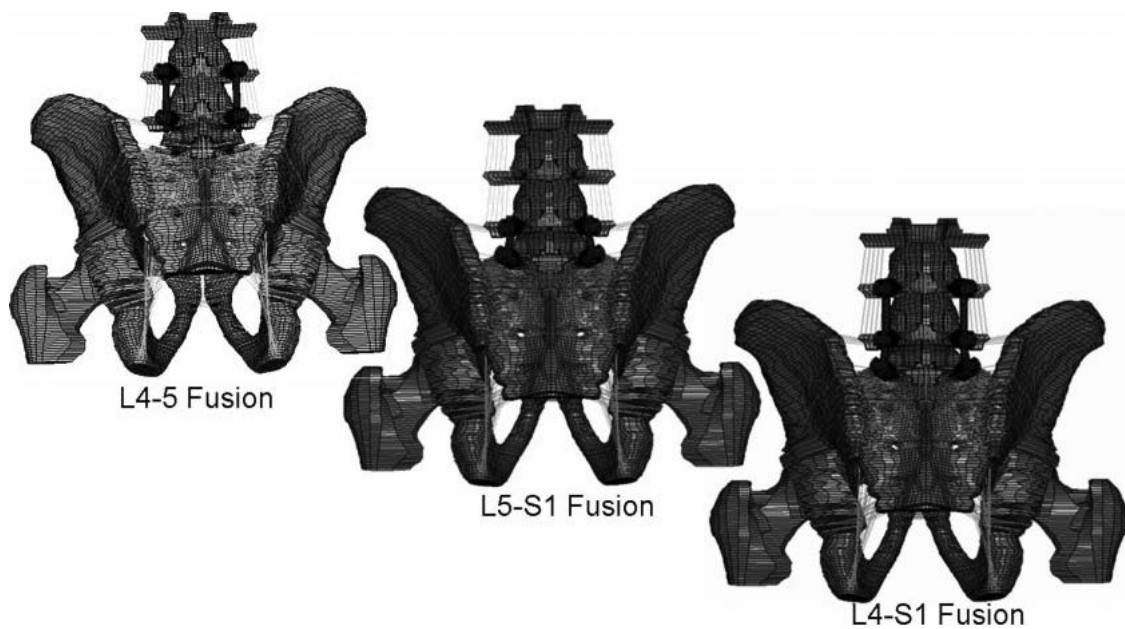


Figure 8. Finite element model with spinal fusions in different levels.⁴⁹

in S2 in both injury types due to placement farther from the S1 endplate. Two screws at S1 and S2 were the strongest placement, compared with placing 2 screws closely in S1 in both dislocation types.

Joukar et al⁵² investigated the effect of unilateral and bilateral SIJ fusion and different placements of fully threaded and half-threaded screws during standing upright (similar to the RI-ALTO and SI-LOK implant systems), on the SIJ male and female models' ROM and stresses (Figure 11). The fully threaded and half-threaded screws were located posterior and lateral into the SIJ, respectively. Unilateral stabilization significantly reduced the fused SIJ ROM along with reduction in contralateral (nonfused) SIJ motion during standing upright. Moreover, regardless of sex, lateral and posterior

placements of the implants had similar performance on the SIJ stability. Both male and female models showed high reduction in stress and ROM after treatment compared with the intact model; however, female model showed more stress and motion reductions after SIJ fusion due to higher stress and ROM values in prior fusion compared to the male model. SIJ implants are more effective in females in terms of stability but may be more prone to higher rate of loosening or failure compared with males. The motion reduction at the SIJ after unilateral and bilateral fusions resulted in minimal changes at the adjacent lumbar levels for both male and female models. Although the implant shape effects were minimal, the implant placements played a major role in stresses on the bone and implant. In both

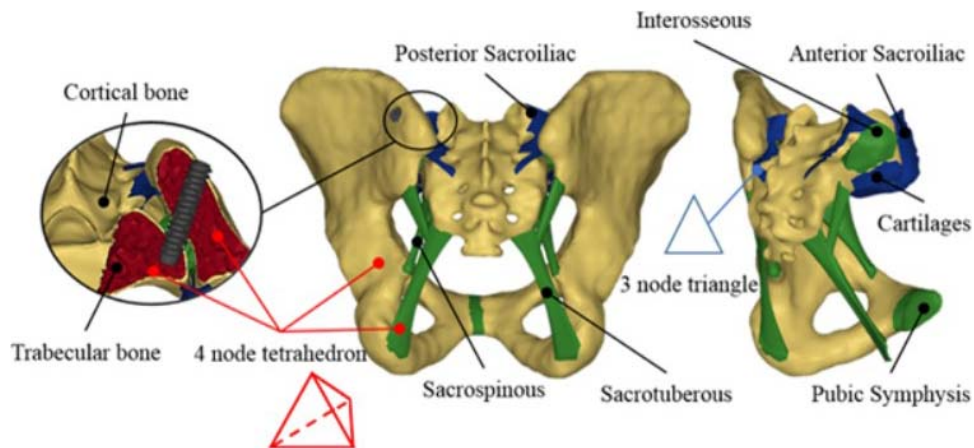


Figure 9. Finite element model of pelvis instrumented with RIALTO implant.⁵⁰

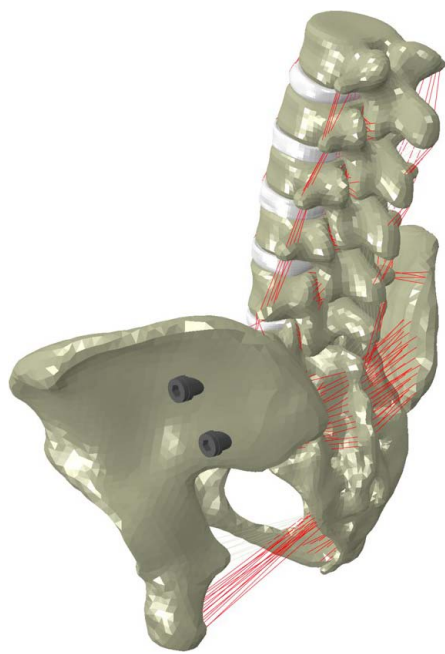


Figure 10. Finite element model of pelvis instrumented with one screw in S1 and another one in S2.⁵¹

unilateral and bilateral fusions, SIJ stabilization was primarily due to the inferior and superior implants.

Lindsey et al⁵³ performed another finite element study on SIJ fusion with triangular implants to assess the biomechanical effects of length, orientation, and number of implants under all 6 spine motions (Figure 12). The following variables were simulated: 1, 2, and 3 implants, superior implant length of 55 mm or 75 mm, midline implant length of 45 mm, and inferior implant length of 45 mm for inline orientation and 50 mm for transarticular orientation. Transarticular orientation provided better fixation compared with inline orientation due to crossing more of the cartilaginous portion of the SIJ, although Soriano-Baron³⁹ revealed that there was no significant difference between these 2 approaches. Use of a longer superior implant led to higher reduction in SIJ motion under different spine motions. In addition, placing 2 implants closer together yielded less stability than 2 implants far from each other. Overall, placing implants in the thicker cortical bone areas and a more dense bone region provided more stability.

In another finite element study by Lindsey et al,⁵⁴ biomechanics of SIJ following various positioning configurations of triangular implants was evaluated. Simulations included altering implant orientation, superior implant length, and number of implants. They predicted that putting 3 implants across the SIJ using a transarticular orientation with the

superior implant closer to the sacral midline led to the most stable construct.

As has been shown earlier, the lumbar segment fusion affects SIJ biomechanics. Lindsey et al⁵³ assessed the ROM of the SIJ and the adjacent lumbar spinal motion segments after SIJ fusion using triangular implants. They showed that SIJ fusion using 3 triangular implants provided a significant reduction in SIJ motion in all 6 motions and resulted in an insignificant increase in adjacent lumbar segment motion.

Joukar et al⁵⁵ developed a validated finite element model of the lumbo-pelvic segment to investigate the biomechanical effects of fixation of sacroiliac joint using triangular implants on the hip joint (Figure 13). Their model included the most critical anatomical features including connective tissue and articular cartilage across the hip joint. They performed an analysis with femurs fixed in a double-leg stance configuration and application of a 400-N compressive follower pre-load applied across the lumbo-sacral segment followed by a 10-Nm bending moment applied to the topmost level of the spine segment. The intact model was modified to include SIJ fixation, and unilateral and bilateral joint instrumentations. The analyses demonstrated a decrease in ROM of the SIJ in the instrumented model, compared with the intact. The bilateral fixation resulted in a greater reduction in motion compared with unilateral fixation. The contact stresses and load sharing did not significantly change in contralateral SIJs following unilateral fixation.

The average hip-contact stress and contact area changed less than 5% and 10%, respectively, in instrumented models relative to intact models in most of anatomical motions. The data suggested a low risk of developing adjacent segment disease across the hip joint due to minimal changes in contact area and load sharing at the hip joint following instrumentation with the triangular implant compared with the intact state. The changes in the lumbar spine segment were minimal as well.

SUMMARY

One of the most overlooked sources of LBP is the SIJ due to its complex nature and the fact that pain emanating from this region can mimic other hip and spine conditions. The first step in the treatment of SIJ dysfunction involves nonsurgical management. When nonsurgical management strategies fail,

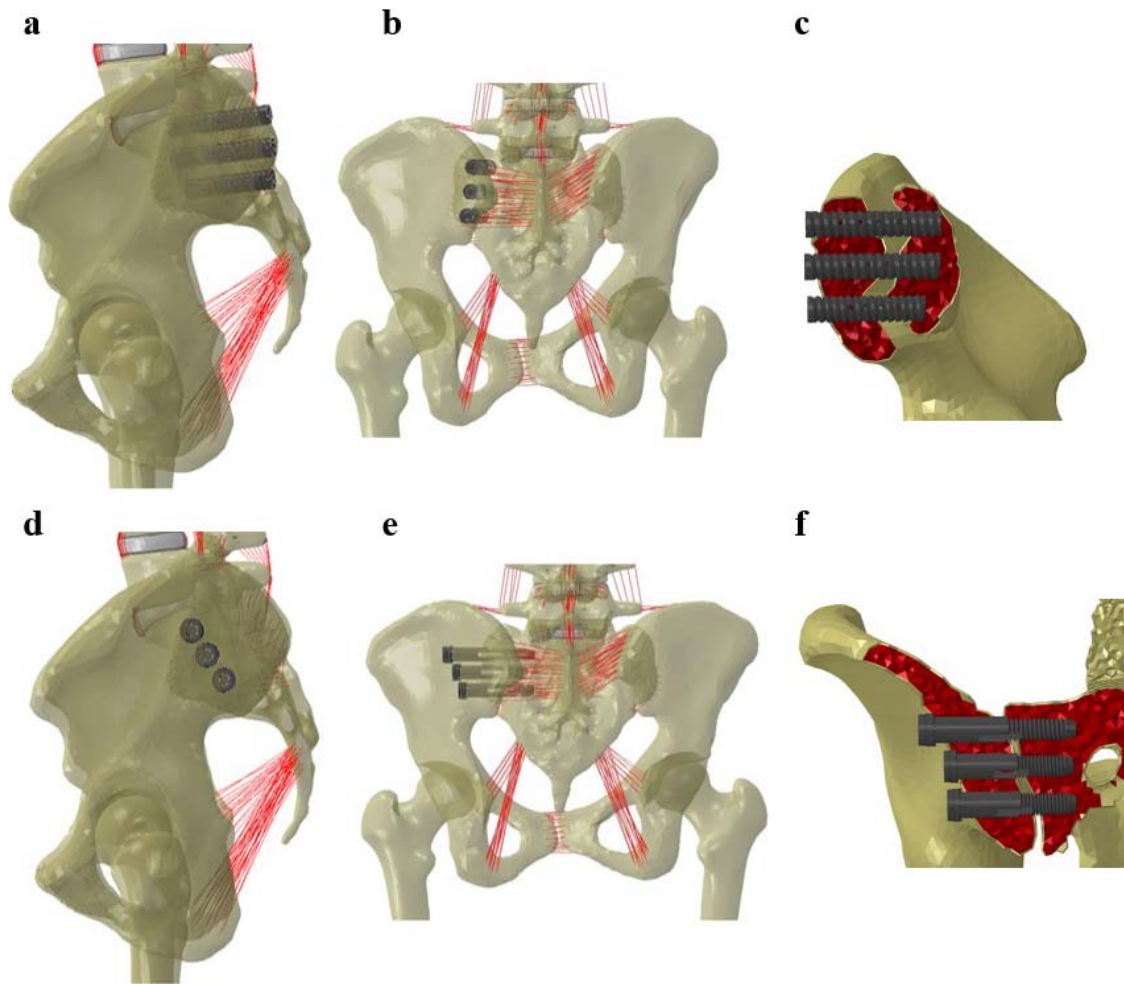
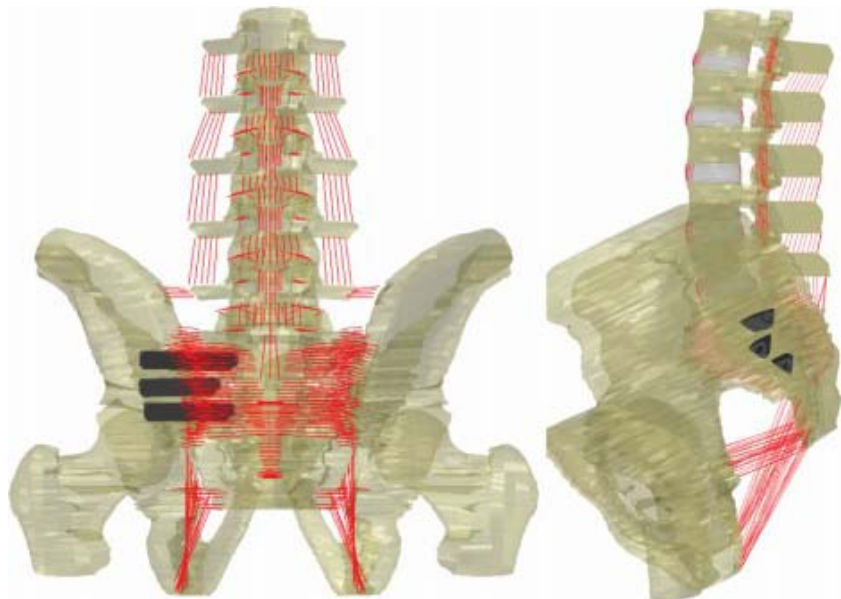


Figure 11. Lateral, posterior, and cross-section views of finite element model instrumented with fully threaded screws (a–c) and lateral, posterior, and cross-section views of finite element model instrumented with half-threaded screws (d–f).⁵²

Figure 12. Finite element spine-pelvis-femur model instrumented with iFuse triangular implants; posterior view (left) and side view (right).⁵³



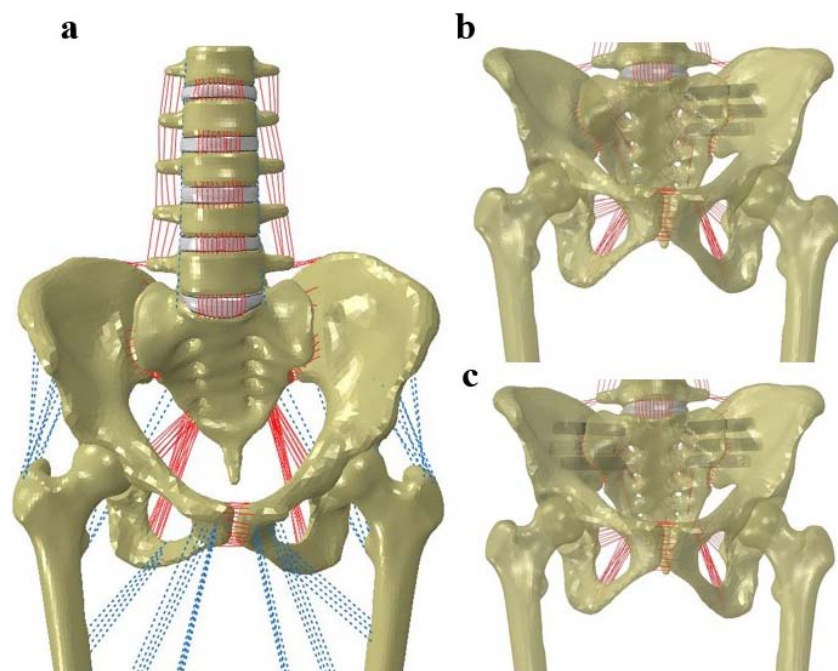


Figure 13. Finite element model of spine-pelvis-femur: intact model including muscles (blue dashed lines), ligaments (red lines) (a); left unilaterally and bilaterally treated models using iFuse implant (b, c).⁵⁵

surgical management (open or minimal fusion) is considered.

Several studies have investigated the clinical outcomes of surgical techniques for the SIJ. The studies have shown that minimally invasive techniques involve less tissue damage, blood loss, and duration of hospitalization, thus leading to superior clinical outcomes.

Despite the satisfactory data on clinical outcomes of SIJ fixation surgery, the data on biomechanics of the SIJ in general and fixation techniques in particular are sparse. The existing literature suggests that at least 2 fixation devices spaced apart in their locations on either side of the pivot point of SIJ facilitates “solid” fixation/stabilization across the joint. However, 1 more implant may further enhance the SIJ fixation. Both unilateral and bilateral SIJ fusions reduce motion. However, if bilateral SIJ fusion is considered, it is essential to ensure that implant design and SIJ morphology permit such a procedure.

Both males and females showed high performance after SIJ fusion treatment; however, females showed greater stress and motion reductions after SIJ fusion. Regardless of sex, lateral and posterior placements of the implants had similar performance on the SIJ stability. SIJ implants are more effective in females in terms of stability but may be more prone to higher rate of loosening or failure compared with males. The optimum number of implants and implant placement location are 2 or 3

implants (depending on the bone quality and implant type) across the S1 and S2 levels of the sacrum. Having implant placement more parallel and farther from the SIJ pivot point results in greater stability of the joint. Using a longer superior implant placed at the S1 level (proximally) closer to the sacral midline leads to greater reduction in SIJ motion. It is better to place the implant in thicker cortical bone areas and a more dense bone region, leading to better stability. Most importantly, SIJ fusion has no effect on the adjacent segments on either side: spine or hip.

Finally, regarding the shapes of the implants, currently there are 2 popular designs on the market: circular sections like SIMmetry, SI-LOK, and RI-ALTO, and a triangular design like iFuse. Further biomechanical studies and long-term clinical follow-ups are required to delineate the optimum design (eg, implant shape) since the existing literature on biomechanics of circular SIJ devices (SIMmetry and SI-LOK implant systems) is limited.

In conclusion, despite the existing literature, there are several unanswered questions related to the effect of surgical parameters on the clinical outcome of the SIJ fixation procedures. For example, the effects of different implant shapes on the biomechanical and long-term clinical outcomes of the SIJ are not fully understood. It is particularly crucial to understand the relationship between bone quality or density and the effectiveness of the surgical technique from a biomechanical perspective, and the

long-term clinical outcomes. Such questions can be answered by looking at parameters such as load-sharing at the bone-implant interface, distribution of the load across the implant, failure mechanism of the bone or implant, and bone remodeling. The clinical studies, due to their inherent limitations, are unable to address such issues. Such knowledge will be crucial for improvement of existing techniques or development of more efficient instrumentation that would yield superior clinical outcomes for SIJ fixation.

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